

James Dargan BMBS,^a, Sam Banisadr, MBChB,^b, Faisal Khan, MBBS,^a, Sami Firoozi, MBBS (Hons),^a, Cameron Dowling, MBBS, PhD,^{c,d}, Stephen J Brecker, MD,^a

^a Cardiovascular clinical academic group, St. George's, University of London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's University Hospitals NHS Foundation Trust, London, UK ^b St. George's UNE St. George's UNE St. Geor UK ^c MonashHeart, Monash Health and Monash Cardiovascular Research Centre, Monash University, Melbourne, Australia ^d Division of Cardiovascular Medicine, Stanford University, Melbourne, Australia ^d Division of Cardiovascular Research Centre, Monash University, Melbourne, Australia ^d Division of Cardiovascular Research Centre, Monash University, Melbourne, Australia ^d Division of Cardiovascular Medicine, Stanford, CA

Background

A difficulty in treating patients with bicuspid aortic valve (BAV) is transcatheter heart valve (THV) sizing due to heterogeneity of bicuspid valve anatomy. In initial studies, this group had a higher rate of complication with more frequent aortic root injury and paravalvular leak (PVL).¹

THV sizing is routinely performed by following a recognised sizing algorithm based on CT-derived data. Complimentary to valve-sizing algorithms is the addition of individualised, patient-specific computer simulation using finite element modelling. This allows for prediction of PVL, conduction disturbance and may yield a different outcome when compared to an algorithmic sizing approach

In this study we aimed to compare the results of the different algorithms in addition to computer modelling in a cohort of patients undergoing TAVI for BAV stenosis.

Methods

A retrospective study was performed on all patients assessed for transcatheter treatment of Sievers Type 1 BAV disease and who had undergone patient specific computer modelling using the FEops HEARTguide platform.

THV sizing was compared using an annular-based sizing algorithm and three BAV sizing algorithms; the Level of Implantation at the Raphe (LIRA), Calcium Algorithm Sizing for Bicuspid Evaluation with Raphe (CASPER) and Bicuspid Aortic Valve Anatomy and Relationship with Devices (BAVARD), yielding both an algorithm-derived diameter and a resulting valve size.²⁻⁴ THV selection was made using the Evolut self-expanding platform, therefore the circle method was not applied.

Patient-specific computer modelling was performed with FEops HEARTguide (FEops, nv, Ghent, Belgium) allowing the selection of the THV which gave the smallest predicted rate of paravalvular leak (PVL).

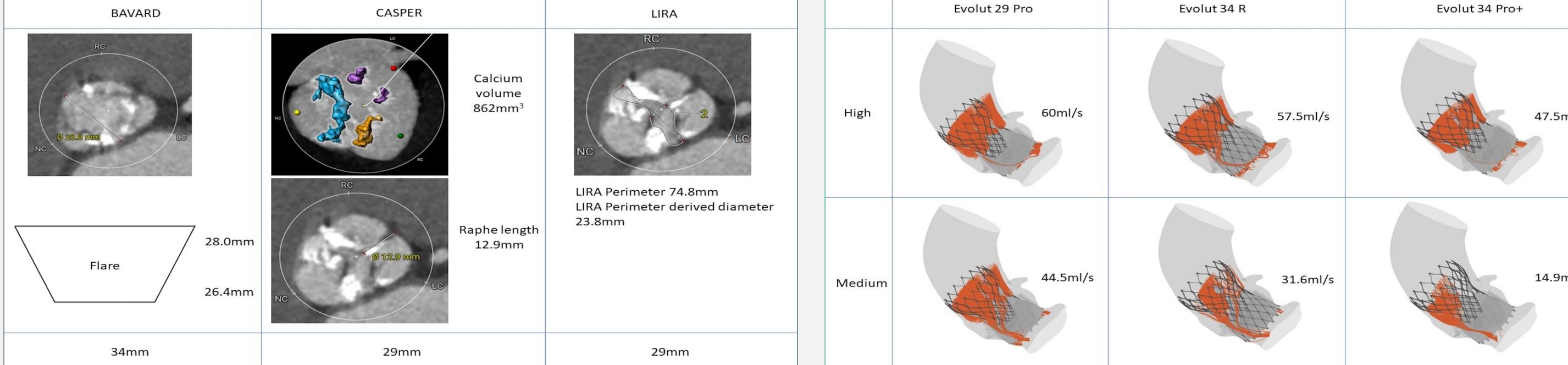
Baseline patient characteristics				
BASELINE CHARACTERISTICS	N = 73			
Age, years	78.1±9.5			
male	48/73 (65.8)			
BMI, kg/m ²	25.6±6.7			
NYHA class III or IV	52/73 (71.2)			
Diabetes Mellitus	15/73 (20.5)			
Known atrial fibrillation	25/73 (34.2)			
Left ventricular ejection fraction, %	51±14.1			
EuroSCORE II, %	3.5±3.1			
STS mortality, %	2.9±1.6			
Presence of coronary artery disease	11/73 (15.1)			
Prior PCI	8/73 (11.0)			
Prior CABG	0/73 (0)			
prior PPM	12/73 (16.4)			
Values are mean±standard deviation or n/N (%)				



Results

A total of 73 patients were included in this study. The mean algorithm-derived diameter for each method was: annular 25.67 mm (25.16-26.18 mm), BAVARD 25.56 mm (25.05-26.06 mm), CASPER 24.1 mm (23.58-24.62 mm) and LIRA 23.46 mm (22.79-24.12 mm). One-way ANOVA demonstrated a significant difference in algorithm-derived diameter (p<0.01), with annular and BAVARD sizing giving a larger diameter than CASPER and LIRA. THV sizing ranged from 23 mm to 34 mm valves. The mean THV size for annular sizing was 31.05 mm (30.34-31.77), BAVARD 30.99 mm (30.27-31.7 mm), FEops 30.27 mm (29.62-30.93 mm), CASPER 29.01 mm (28.34-29.68 mm) and LIRA 28.36 mm (27.58-29.13 mm) One-way ANOVA showed a significant difference in THV sizing (p<0.01), forming 3 groups; group 1: Annular, BAVARD and FEops, group 2: FEops and Casper, and group 3: CASPER and LIRA. Group 1 resulted in the largest THV size and group 3 the smallest.

In 74% of patients (n=54) there was variation in THV sizing across the different algorithms. In 14.2% of patients (n=11) there was a difference of 2 THV sizes between algorithms.



Patient-specific computer simulation and valve-sizing methods in bicuspid TAVI

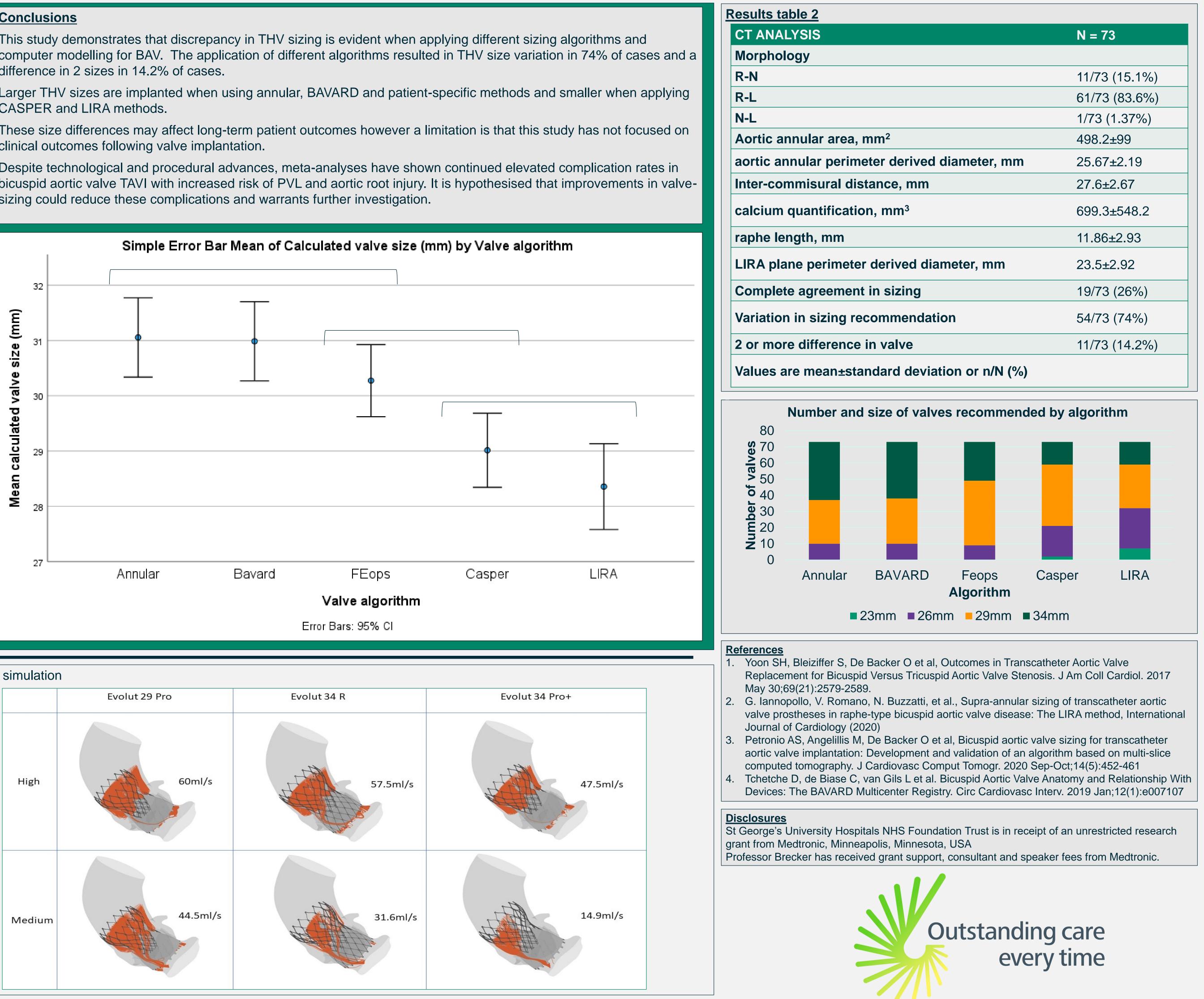
mple Error Bar Mear	n of Calculated perimet	er derived diameter by \	/alve algorithm	-
				-
		•		[
Annular	Bavard	Casper	LIRA	
	Valve a	lgorithm		
	Error Bars: 9	5% CI		

Figure 1: demonstrating a worked example of application of the different valve algorithms and patient-specific computer simulation

difference in 2 sizes in 14.2% of cases.

CASPER and LIRA methods.

clinical outcomes following valve implantation.



NHS St George's University Hospitals **NHS Foundation Trust**